

Edition 2.0 2022-07

TECHNICAL SPECIFICATION



Ultrasonics – Pulse-echo scanners – Low-echo sphere phantoms and method for performance testing of grey-scale medical ultrasound scanners applicable to a broad range of transducer types

INTERNATIONAL ELECTROTECHNICAL COMMISSION

ICS 11.040.50; 17.140.50

ISBN 978-2-8322-3922-3

Warning! Make sure that you obtained this publication from an authorized distributor.

CONTENTS

FOREWORD	6
INTRODUCTION	8
1 Scope	10
2 Normative references	10
3 Terms and definitions	11
4 Symbols	15
5 General and environmental conditions	
6 Equipment required	17
6.1 General	
6.2 Phantom geometries	
6.2.1 Low-contrast phantoms for assessing the ability to delineate tumour boundaries	
6.2.2 High-contrast phantoms to evaluate scanner performance, tune scanner pre-sets, and detect defects in probes	18
6.2.3 Total internal reflection surfaces	
6.2.4 Spatially random distribution of low-echo spheres	
6.3 Ultrasonic properties of the tissue-mimicking (TM) phantoms	
7 Data acquisition assuming a spatially random distribution of low-echo spheres	
7.1 Methodology	
7.1.1 General	
7.1.2 Mechanical translation	
 7.1.3 Manual translation with cine-loop recording 7.2 Storage of digitized image data 	
7.2 Storage of digitized image data7.3 Digital image files available from the scanner itself	
7.4 Image archiving systems	
8 Automated data analysis for quantifying low-echo sphere detectability	
8.1 General	
8.2 Computation of mean pixel values (<i>MPV</i> s)	
8.3 Additional restrictions for sector images	
8.3.1 Convex arrays	
8.3.2 Phased arrays	30
8.4 Determination of the <i>LSNR</i> _m -value for a given depth interval	30
8.4.1 Preliminaries	30
8.4.2 Computation of <i>LSNR</i> _{md} for depth interval label <i>d</i>	31
8.4.3 Standard error corresponding to each <i>LSNR</i> _{md} -value	31
9 Visual assessments of images	
9.1 Image comparisons	
9.2 Semi-quantitative image analysis	
Annex A (informative) Example of a phantom for performance testing in the 1 MHz to 7 MHz frequency range	
Annex B (informative) Illustrations of the computation of <i>LSNR</i> _{md} -values as a function	
of depth	36
Annex C (informative) Sufficient number of data images to assure reproducibility of results	43
C.1 General	

C.2	Phantom with 3,2-mm-diameter, -20 dB low-echo sphere, having two spheres per millilitre	43
C.3	Phantom with 2-mm-diameter, −20 dB spheres and eight spheres per millilitre	48
	(informative) Example of a phantom for performance testing in the 7 MHz to requency range	52
Annex E	(informative) Determination of low-echo sphere positions to within $D/8$ in x-, Cartesian coordinates	
E.1	Procedure	
E.2	Argument for the choice of seven <i>MPV</i> nearest-neighbour sites for determining the centres of low-echo spheres	
	(informative) Tests of total internal reflection produced by alumina and plate- ine reflectors	
Annex G	(informative) Results of a test of reproducibility of <i>LSNR_{md}</i> as a function of	
depth for	a phantom with 4-mm-diameter, -20 dB spheres, having two spheres per	64
	(informative) Results for low-echo sphere concentration dependence of as a function of depth for phantoms with 3,2-mm-diameter, −20 dB spheres	66
	informative) Comparison of two different makes of scanner with similar ers and console settings	70
Annex J (informative) Special considerations for 3-D probes	72
J.1	3-D probes operating in 2-D imaging mode	72
J.2	2-D arrays operating in 3-D imaging mode for determining <i>LSNR</i> _{md} -values as	
	a function of depth for reconstructed images	
J.3	Mechanically driven 3-D probes operating in 3-D imaging mode	
Bibliograp	bhy	73
-	- Flow chart	22
	- Schematic of the image plane nearest to the <i>n</i> th low-echo sphere and not d by the presence of an image boundary	25
	- Modification of Figure 2 showing a vertical image boundary (solid line) and dashed line, between which $(MPV)_{ijk}$ values are excluded from computation	
of S_{mBn} of	or σ_{Bn} in Formula (2)	26
	 Limiting case of Figure 3 where the vertical image boundary is tangent to ad low-echo sphere 	27
	– Modification of Figure 2 showing a 45° sector image boundary (solid line) allel dashed line, between which $(MPV)_{iik}$ values are excluded from	
	ion of S_{mBn} or σ_{Bn} in Formula (2)	28
Figure 6 -	 Limiting case of Figure 5 where the 45° sector image boundary is tangent to ad low-echo sphere 	
Figure 7 -	- Usefulness of simple visual inspection of images of a standardized low-echo nantom	
Figure 8 - nearly ful	- Zones over which at least half of the spheres appear clearly outlined as a I-size circle and are free of echoes (Zone 1) or an average of more than one er slice can be discerned (Zone 2)	
	1 – End view of the phantom applicable for 1 MHz to 7 MHz showing the random distribution of 3,2-mm-diameter, -6 dB spheres	34
Figure A.	2 – Top view of phantom with 3,2-mm-diameter, −6 dB spheres	35
Figure B.	1 – Convex-array image of a prototype 4-mm-diameter, −20 dB sphere for use in the 1 MHz to 7 MHz frequency range	
pnantom		

Figure B.2 – Auxiliary figures relating to Figure B.1	37
Figure B.3 – Results corresponding to Figure B.1 and Figure B.2, demonstrating reproducibility	38
Figure B.4 – Results corresponding to Figure B.1, Figure B.2 and Figure B.3	39
Figure B.5 – One of 80 parallel, linear-array images of the phantom containing 4-mm-diameter, -20 dB spheres, imaged at 4 MHz with the transmit focus at 3 cm depth	39
Figure B.6 – Three successive images of the set of 80 frames addressed in Figure B.5, where imaging planes were separated by $D/4$ equal to 1 mm	40
Figure B.7 – Results for the 4-cm-wide, 3-cm-focus, linear array addressed in Figure B.5 and Figure B.6 using all 80 image frames in two sets	41
Figure B.8 – Results for the 4-cm-wide, 3-cm-focus, linear array addressed in Figure B.5, Figure B.6 and Figure B.7, using all 80 image frames corresponding to Figure B.7 in one set	42
Figure C.1 – One image obtained from a phantom containing 3,2-mm-diameter, −20 dB spheres by using a 4 MHz linear array focused at 3 cm depth	43
Figure C.2 – Reproducibility result for two independent sets of 70 images with a mean number of low-echo sphere centres that is about 15 per 5 mm-depth interval	44
Figure C.3 – Results obtained by combining both sets of 70 independent images corresponding to Figure C.2 into a single, 140-image set	45
Figure C.4 – Sector image (curved array) at 4,5 MHz with multiple transmit foci at 4 cm, 8 cm and 12 cm depths; the -20 dB spheres are 3,2 mm in diameter	45
Figure C.5 – Reproducibility results for a multiple transmit-focus (4 cm, 8 cm and 12 cm) case corresponding to Figure C.4	46
Figure C.6 – Reproducibility results for the case corresponding to Figure C.5, except that there is a single focus at a 10 cm depth	47
Figure C.7 – Reproducibility results for the case corresponding to Figure C.5, except that there is a single transmit focus at 4 cm depth	47
Figure C.8 – Image of a phantom containing 2-mm-diameter, -20 dB spheres, made with a curved array having a 1,5 cm radius of curvature, with its transmit focus at 3 cm depth	48
Figure C.9 – Reproducibility results corresponding to Figure C.8	49
Figure C.10 – Results using all 100 images in the image set that gave rise to Figure C.9	49
Figure C.11 – Image of a phantom containing 2-mm-diameter, -20 dB spheres, made with a high-frequency (15 MHz) linear array and a transmit focus of 4 cm depth	50
Figure C.12 – Reproducibility results corresponding to Figure C.11	51
Figure C.13 – Results using all 200 images in the image set that gave rise to Figure C.12	51
Figure D.1 – End- and top-view diagrams of the phantom containing 2-mm-diameter, low-echo spheres with a backscatter level -20 dB relative to the background, for use in the 7 MHz to 23 MHz frequency range	52
Figure D.2 – Image of the phantom containing 2-mm-diameter, -20 dB spheres [7], [8] obtained with a paediatric transducer with a radius of curvature of about 1,5 cm	53
Figure E.1 – Diagram discussed in the second paragraph of 3)	54
Figure F.1 – Average of 10 images obtained by using a phased array transducer	58
Figure F.2 – Mean and standard deviation of pixel value plotted against depth from the two rectangular regions seen in Figure F.1	59
Figure F.3 – Same as Figure F.2, but for data obtained after the transducer was rotated 180°, so the plate-glass reflector appeared on the right side of the image	59

Figure F.4 – The percentage by which the mean pixel values resulting from reflections differ from the mean pixel values not involving reflections plotted against depth60
Figure F.5 – Image obtained using a wide-sector (153°), 1 cm radius-of-curvature transducer
Figure F.6 – Mean pixel value and its standard deviation plotted against depth from the two rectangular regions in Figure F.5
Figure F.7 – Same as Figure F.6, only the transducer was rotated 180°, so the alumina reflector was on the right side of the B-mode image
Figure F.8 – The percentage by which the mean pixel values resulting from reflections differ from the mean pixel values not involving reflections
Figure G.1 – Example image of the phantom, taken with a 4,2 MHz curved array64
Figure G.2 – Reproducibility results corresponding to the two 40-image data subsets, one of which is shown in Figure G.1
Figure H.1 – Example of an image from the 75-image, 4 ml ⁻¹ data set producing the results shown in Figure H.2
Figure H.2 – Results for the phantom containing four 3,2-mm-diameter, -20 dB low- echo spheres per millilitre
Figure H.3 – Example of an image from the 140-image, two spheres per millilitre data set producing the results shown in Figure H.467
Figure H.4 – Results for the phantom containing two 3,2-mm-diameter, −20 dB low- echo spheres per millilitre
Figure H.5 – Example of an image from the 180-image, one sphere per millilitre data set producing the results shown in Figure H.6
Figure H.6 – Results for the phantom containing one 3,2-mm-diameter, −20 dB low- echo sphere per millilitre
Figure I.1 – Results for System A scanner and 7CF2 3-D (swept convex array) transducer focused at 4 cm depth and operated at 4,5 MHz in 2-D mode
Figure I.2 – Results for System B scanner with a 4DC7-3 3-D (convex array) transducer focused at 4 cm depth and operated at 4 MHz in 2-D mode71

INTERNATIONAL ELECTROTECHNICAL COMMISSION

ULTRASONICS – PULSE-ECHO SCANNERS – LOW-ECHO SPHERE PHANTOMS AND METHOD FOR PERFORMANCE TESTING OF GREY-SCALE MEDICAL ULTRASOUND SCANNERS APPLICABLE TO A BROAD RANGE OF TRANSDUCER TYPES

FOREWORD

- 1) The International Electrotechnical Commission (IEC) is a worldwide organization for standardization comprising all national electrotechnical committees (IEC National Committees). The object of IEC is to promote international co-operation on all questions concerning standardization in the electrical and electronic fields. To this end and in addition to other activities, IEC publishes International Standards, Technical Specifications, Technical Reports, Publicly Available Specifications (PAS) and Guides (hereafter referred to as "IEC Publication(s)"). Their preparation is entrusted to technical committees; any IEC National Committee interested in the subject dealt with may participate in this preparatory work. International, governmental and non-governmental organizations liaising with the IEC also participate in this preparation. IEC collaborates closely with the International Organization for Standardization (ISO) in accordance with conditions determined by agreement between the two organizations.
- The formal decisions or agreements of IEC on technical matters express, as nearly as possible, an international consensus of opinion on the relevant subjects since each technical committee has representation from all interested IEC National Committees.
- 3) IEC Publications have the form of recommendations for international use and are accepted by IEC National Committees in that sense. While all reasonable efforts are made to ensure that the technical content of IEC Publications is accurate, IEC cannot be held responsible for the way in which they are used or for any misinterpretation by any end user.
- 4) In order to promote international uniformity, IEC National Committees undertake to apply IEC Publications transparently to the maximum extent possible in their national and regional publications. Any divergence between any IEC Publication and the corresponding national or regional publication shall be clearly indicated in the latter.
- 5) IEC itself does not provide any attestation of conformity. Independent certification bodies provide conformity assessment services and, in some areas, access to IEC marks of conformity. IEC is not responsible for any services carried out by independent certification bodies.
- 6) All users should ensure that they have the latest edition of this publication.
- 7) No liability shall attach to IEC or its directors, employees, servants or agents including individual experts and members of its technical committees and IEC National Committees for any personal injury, property damage or other damage of any nature whatsoever, whether direct or indirect, or for costs (including legal fees) and expenses arising out of the publication, use of, or reliance upon, this IEC Publication or any other IEC Publications.
- 8) Attention is drawn to the Normative references cited in this publication. Use of the referenced publications is indispensable for the correct application of this publication.
- 9) Attention is drawn to the possibility that some of the elements of this IEC Publication may be the subject of patent rights. IEC shall not be held responsible for identifying any or all such patent rights.

IEC TS 62791 has been prepared by IEC technical committee 87: Ultrasonics. It is a Technical Specification.

This second edition cancels and replaces the first edition published in 2015. This edition constitutes a technical revision.

This edition includes the following significant technical changes with respect to the previous edition.

- a) It introduces necessary corrections to the analysis methods; these have been published in the literature.
- b) It increases the range of contrast levels of **low-echo spheres** in phantoms that meet this Technical Specification. Previous specification was -20 dB, but two additional levels, -6 dB and either -30 dB or, if possible, -40 dB, are now specified.
- c) It includes a wider range of uses of the methodology, including testing the effectiveness of scanner pre-sets for specific clinical tasks and detecting flaws in transducers and in beamforming.

d) It decreases the manufacturing cost by decreasing phantoms' dimensions and numbers of low-echo, backscattering spheres embedded in each phantom.

The text of this Technical Specification is based on the following documents:

Draft	Report on voting
87/776/DTS	87/790A/RVDTS

Full information on the voting for its approval can be found in the report on voting indicated in the above table.

The language used for the development of this Technical Specification is English.

This document was drafted in accordance with ISO/IEC Directives, Part 2, and developed in accordance with ISO/IEC Directives, Part 1 and ISO/IEC Directives, IEC Supplement, available at www.iec.ch/members_experts/refdocs. The main document types developed by IEC are described in greater detail at www.iec.ch/standardsdev/publications.

Terms in **bold** in the text are defined in Clause 3.

The committee has decided that the contents of this document will remain unchanged until the stability date indicated on the IEC website under webstore.iec.ch in the data related to the specific document. At this date, the document will be

- reconfirmed,
- withdrawn,
- replaced by a revised edition, or
- amended.

IMPORTANT – The "colour inside" logo on the cover page of this document indicates that it contains colours which are considered to be useful for the correct understanding of its contents. Users should therefore print this document using a colour printer.

INTRODUCTION

Ultrasonic pulse-echo scanners are widely used in medical practice to produce images of softtissue organs throughout the human body. Most ultrasonic pulse-echo scanners produce realtime images of tissue in a scan plane by sweeping a narrow, pulsed beam of ultrasound through the tissue section of interest and detecting the echoes generated by reflection at tissue boundaries and by scattering within tissues. Many newer scanners transmit broad, overlapping ultrasound beams, and apply software beam-forming to synthesize narrow, pulse-echo beam patterns.

Generally, the sweep that generates an image frame is repeated at least 20 times per second, giving rise to the real-time aspect of the displayed image. The axes of the pulsed beams generally lie in a plane that defines the scan plane.

Various transducer types are employed to operate in a transmit–receive mode to generate and detect the ultrasonic signals. Linear arrays, in which the beam axes are all parallel to one another, resulting in a rectangular image, consist of a line of hundreds of parallel transducer elements with a subset of adjacent elements producing one pulse at a time. Convex arrays are similar to linear arrays but the element arrangements define part of the surface of a short, right, circular cylinder with the array elements parallel to the axis of the cylinder. The radius of curvature of the cylinder (and therefore the array) can have values between 0,5 cm and 7 cm. The convex array generates a sector image, since the beam axes fan out over the scan plane. Some linear- and convex-array models, such as "1,25-D" arrays, incorporate multiple rows of elements to provide additional control of the elevational beam width.

A phased array has a linear arrangement of elements, where all elements act together to form a pulse and the direction and focus of an emitted pulse is determined by the timing of excitations of the elements. The phased array generates a sector image. Another type of sector scanner is the mechanical sector scanner in which a single-element transducer or an annular-array transducer is rotated about a fixed axis during pulse emissions. The foregoing transducer types commonly operate within the frequency range 1 MHz to 23 MHz, to which this document applies. Medical ultrasound systems exist whose transducers operate at frequencies as high as 33 MHz. Although the procedures specified in this document might be appropriate for these systems, phantoms outlined in this document have not yet been described for use in the 23 MHz to 33 MHz frequency range.

A two-dimensional array (2-D array) is restricted to an array of transducer elements distributed over a rectangular area or a spherical cap. Such an array receives echoes from a 3-D volume and can produce images corresponding to any planar surface in that volume. A 3-D mechanically driven, convex array (3-D MD convex array) means a convex array that acquires images as it is rotated mechanically about an axis lying in its **image plane** or an extension of that plane. A 3-D mechanically driven, linear array (3-D MD linear array) is similar to a 3-D MD convex array, where the array radius of curvature is infinite and the array is either rotated about an axis or is translated perpendicularly to the scan plane of the linear array. For an overview of current 3-D and 4-D systems, see 1.5 and 10.2.2 of [1]¹.

One means for testing the imaging performance of an ultrasound pulse-echo scanner is to quantify the degree to which a small (low-echo) sphere is distinguished from the surrounding soft tissue, i.e. the degree to which a small, **low-echo sphere** is detectable in the surrounding soft tissue. It is reasonable to assume that the smaller the **low-echo sphere** that can be detected at some position, the better the resolution of the scanner, i.e. the better it will display and delineate the boundary of an abnormal object, such as a tumour, and the more accurately it will display local acoustic properties.

¹ Numbers in square brackets refer to the Bibliography.

- 9 -

There are three components of resolution defined in pulse-echo ultrasound:

- axial resolution (parallel to the local, pulse-propagation direction);
- lateral resolution (perpendicular to the local, pulse-propagation direction and parallel to the scan plane); and
- elevational resolution (perpendicular to the local, pulse-propagation direction and also to the scan plane).

Axial resolution usually – but not always – is better than lateral and elevational resolutions. Thus, all three components affect an object's **detectability**. A sphere has no preferred orientation and is therefore the best shape for assessing **detectability** of a low-echo object for two reasons. First, all three components of resolution are weighted equally, no matter what the beam's incident direction is. Second, the incident beam's propagation direction will vary considerably in the case of convex and phased arrays depending on where the object exists in the imaged volume.

Imaging performance can be reduced by:

- beam distortions associated with dead or weak elements in array transducers;
- side lobes and grating lobes that are present with some array transducers;
- unexpected beam changes accompanying variations in the transmit foci applied to multi-row ("1,25-D") arrays; and
- electronic noise.

All can contribute to artifactual echoes on clinical images and on images of phantoms containing **low-echo spheres** or to erroneous echo-signal amplitudes.

It is important that the phantom allow quantification of **detectability** to be carried out over the entire depth range imaged; thus, it is important that the **low-echo spheres** exist up to the entire scanning window. A phantom limited to a flat scanning surface is acceptable for a linear array, phased array or a flat 2-D array but not for the remaining types of arrays. Each of the phantoms specified in this document contains a random distribution of equal diameter [2], **low-echo spheres** existing at all depths, including the case of those designed for testing convex (curved) arrays.

This document summarizes the requirements for a phantom to provide for determination of **detectability** of small, **low-echo spheres** for any type of pulse-echo transducer, except (perhaps) a 2-D array with a spherical-cap surface.

The International Electrotechnical Commission (IEC) draws attention to the fact that it is claimed that compliance with this document may involve the use of a patent. IEC takes no position concerning the evidence, validity, and scope of this patent right.

The holder of this patent right has assured IEC that s/he/it is willing to negotiate licences under reasonable and non-discriminatory terms and conditions with applicants throughout the world. In this respect, the statement of the holder of this patent right is registered with IEC. Information can be obtained from the patent database available at patents.iec.ch.

Attention is drawn to the possibility that some of the elements of this document may be the subject of patent rights other than those in the patent database. IEC shall not be held responsible for identifying any or all such patent rights.

ULTRASONICS – PULSE-ECHO SCANNERS – LOW-ECHO SPHERE PHANTOMS AND METHOD FOR PERFORMANCE TESTING OF GREY-SCALE MEDICAL ULTRASOUND SCANNERS APPLICABLE TO A BROAD RANGE OF TRANSDUCER TYPES

1 Scope

This document, which is a Technical Specification, defines terms and specifies methods for quantifying detailed imaging performance of real-time, ultrasound B-mode scanners. Detail is assessed by imaging phantoms containing small, low-echo spherical targets in a tissuemimicking background and analysing sphere **detectability** [3]. Specifications are given for phantom properties. In addition, procedures are described for acquiring images, conducting qualitative analysis of sphere **detectability**, and carrying out quantitative analysis by detecting sphere locations and computing their contrast-to-noise ratios. With appropriate choices in design, results can be applied, for example:

- to assess the relative ability of scanner configurations (scanner make and model, scan head and console settings) to delineate the boundary of a tumour or identify specific features of tumours;
- to choose scanner control settings, such as frequency or the number and location of transmit foci, which maximize spatial resolution;
- to detect defects in probes causing enhanced sidelobes and spurious echoes.

The types of transducers used (see sections 7.6 and 10.7 of [1]) with these scanners include:

- a) phased arrays,
- b) linear arrays,
- c) convex arrays,
- d) mechanical sector scanners,
- e) 3-D probes operating in 2-D imaging mode, and
- f) 3-D probes operating in 3-D imaging mode for a limited number of sets of reconstructed 2-D images.

The test methodology is applicable for transducers operating in the 1 MHz to 23 MHz frequency range.

2 Normative references

The following documents are referred to in the text in such a way that some or all of their content constitutes requirements of this document. For dated references, only the edition cited applies. For undated references, the latest edition of the referenced document (including any amendments) applies.

IEC 60050-802, International Electrotechnical Vocabulary – Ultrasonics (available at: http://www.electropedia.org)

IEC 61391-1, Ultrasonics – Pulse-echo scanners – Part 1: Techniques for calibrating spatial measurement systems and measurement of system point-spread function response

IEC 61391-2:2010, Ultrasonics – Pulse-echo scanners – Part 2: Measurement of maximum depth of penetration and local dynamic range

IEC TS 62736, Ultrasonics – Pulse-echo scanners – Simple methods for periodic testing to verify stability of an imaging system's elementary performance